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Development and applications of a model for cellular response to multiple chemotactic cues

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Abstract. The chemotactic response of a cell population to a single chemical species has been characterized experimentally for many cell types and has been extensively studied from a theoretical standpoint. However, cells frequently have multiple receptor types and can detect and respond chemotactically to more than one chemical. How these signals are integrated within the cell is not known, and we therefore adopt a macroscopic phenomenological approach to this problem. In this paper we derive and analyze chemotactic models based on partial differential (chemotaxis) equations for cell movement in response to multiple chemotactic cues. Our derivation generalizes the approach of Othmer and Stevens [29], who have recently developed a modeling framework for studying different chemotactic responses to a single chemical species. The importance of such a generalization is illustrated by the effect of multiple chemical cues on the chemotactic sensitivity and the spatial pattern of cell densities in several examples. We demonstrate that the model can generate the complex patterns observed on the skin of certain animal species and we indicate how the chemotactic response can be viewed as a form of positional indicator.

1. Introduction

A characteristic feature of a wide variety of living organisms is that they can alter their motile behavior in response to external environmental cues and, in particular, to chemical stimuli. Examples range over many orders of magnitude in spatial scale. The green turtle, *Chelonia mydas* travels over 1000 miles to its breeding ground, through detection of an unknown chemical source originating there [19] and species of shark have the ability to detect traces of blood miles from an injured animal. At the other extreme, fibroblast cells are thought to move into wounds in response to chemical signals emitted at the wound site, and in cellular slime mold

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Dictyostelium discoideum, amoebae respond to the chemoattractant cAMP over spatial scales of the order of a cell diameter [28].

The directed motile response of organisms to chemical cues is called *chemotaxis*. Frequently this individual response is manifested at the population level by the collective movement of a population up (or down) a gradient in concentration of a *chemoattractant* (or *chemorepellent*). Organisms also rely on other forms of taxis for guidance, including light (phototaxis), electric fields (galvanotaxis), magnetic fields (magnetotaxis), and adhesive gradients (haptotaxis). Smaller organisms such as bacteria frequently rely on some form of *kinesis*, which involves modulation of either the speed or the duration of movement in response to environmental conditions. Both taxes and kineses can often be described by similar macroscopic equations, called chemotaxis equations (to be discussed later), even though the stochastic processes that describe movement at the single-organism level may be quite different. Thus one frequently lumps macroscopic descriptions of both taxes and kineses together under the general heading of taxes.

Chemotaxis in bacterial species such as *E. coli* and *S. typhimurium* has been extensively studied both experimentally and theoretically. *E. coli* cells move by rotating rigid helical flagella in a corkscrew-like manner [32]. Each cell contains 6–8 flagella distributed uniformly over the cell surface [37], which, when rotated counterclockwise, coalesce into a propulsive bundle, resulting in a relatively straight “run” [5]. When rotated clockwise they fly apart, resulting in a “tumble” which reorients the cell but causes no significant translocation. The cell thus alternates between runs and reorienting tumbles. In the absence of stimuli, the probability per unit time of a tumble is essentially independent of when the last tumble occurred [37]. In a chemoeffector gradient, the cell carries out chemotactic migration by extending runs that carry it in favorable directions. Using specific chemoreceptors to monitor its chemical environment, *E. coli* perceives spatial gradients as temporal changes in attractant or repellent concentration. The cell in effect compares its environment during the past second with the previous 3–4 seconds and responds accordingly. Attractant increases and repellent decreases transiently raise the probability of CCW rotation, or ‘bias’, and then a sensory adaptation process returns the bias to baseline, enabling the cell to detect and respond to further concentration changes [36]. Attractants include sugars, amino acids and small peptides, and negative chemotaxis (repulsion) occurs in response to noxious substances.

The chemotactic response of cells to a single attractant or repellent has been characterized experimentally for many cell types and has been extensively studied from a theoretical standpoint [30, 28]. However, many cell types have multiple receptor types and can detect and respond chemotactically to more than one chemical. For example, in wiring the nervous system of a developing embryo, tight directional control of the growth of axons is needed in order to ensure that they connect properly with nerve cells, muscles and other tissues. The four principal cues involved are short range (surface) attractants and repellents and long range (diffusive) attractants and repellents. Many diffusible attractants and repellents have been discovered, principally Netrin-1 [33] and members of the semaphorin families [12], [22]. While it functions as an attractant for certain types of axons, Netrin-1 also serves as a repellent for other types [7]. It is believed that many chemicals are

involved in guidance, and that each type of molecule attracts some axons and repels others.

Chemotaxis has also been widely-studied in the clinical sciences because it is an important component of certain aspects of the immune response. Chemattractants released at the site of an infection attract white blood cells in the first response [1], and it has recently been found that adaptation plays an important role in guiding leukocytes through the attractant landscape set up by spatially-separated sources [15]. In tumor-induced angiogenesis, cancerous cells secrete chemoattractants into the surrounding tissue, stimulating endothelial cells in neighboring blood vessels to migrate towards the tumor, thus creating a blood vessel link to the tumor. Several chemoattractants (or tumor angiogenic factors) have been identified, including basic fibroblast growth factor, angiogenin and vascular endothelial growth factor.

Despite the evidence showing that cells respond chemotactically to multiple environmental cues, mathematical models and experimental studies typically focus on the response to a single stimulus. However, the presence of multiple chemotactic signals raises a number of important questions, *viz.*,

- How are the multiple signals integrated intracellularly and interpreted to initiate movement? For example, how is the occupancy of different receptor types in a bacterium integrated and transduced into a response? It is known that the chemotactic protein $CheY_p$ modulates the rotational bias of a flagellar motor, and thus signal integration is easy for pathways using the same chemotaxis proteins, but how is it done when different receptor types generate different signal types?
- What effects do competing attractant and/or repellent signals have on macroscopic spatial patterns? For example, bacteria form a variety of intricate spatial patterns under different nutrient levels [4,38,3,6] but little is known as to whether these patterns depend significantly on the presence of multiple signals, and whether simple changes in the balance between different signals can account for observed changes in the pattern types.
- How is information filtered and processed by the organism? If signals of different magnitudes (e.g. in gradient strength or concentration level), or of different spatial and temporal scales are detected, how can an organism process the information so as to generate the optimal response? This question may be particularly relevant in ecology, where multiple signaling cues can vary on different spatial scales.

These questions have not been answered at the molecular or higher level in any system, and therefore we adopt a more phenomenological approach here. We begin with a master equation for a stochastic space jump process and reduce this to a partial differential equation to describe the movement of organisms in response to multiple tactic signals. We derive a number of forms for the chemotactic sensitivity (defined later), based on how information external to the organism is detected and transduced to result in movement, and we investigate in detail spatial patterning in a simple model for a cell population responding to two competing attractants.

Applications of the work are considered in bacterial cell movement and the complicated pigmentation patterns seen on the skins of certain animals.

How these signals are integrated within the cell is not known, and we therefore adopt a macroscopic phenomenological approach to this problem. In this paper we derive and analyze chemotactic models based on partial differential (chemotaxis) equations for cell movement in response to multiple chemotactic cues.

2. Modeling the tactic response to multiple signals

Othmer and Stevens [29] investigated continuum limits of a continuous time, discrete space random walk described by a master equation, in which walkers execute instantaneous jumps in space at random times. In their analysis, which was motivated by results of Davis [8] on reinforced random walks, the transition probabilities depend on a control substance that itself evolves in time and space. In the following we begin with the same master equation, but now under the assumption that the transition rate is dependent on multiple signals.

Suppose that the probability that a walker is at $n \in \mathbb{Z}$ at time t , given that the walk begin at 0 at $t = 0$, is given by $p_n(t)$. By hypothesis this satisfies the evolution equation

$$\frac{\partial p_n}{\partial t} = \mathcal{T}_{n-1}^+(U)p_{n-1} + \mathcal{T}_{n+1}^-(U)p_{n+1} - (\mathcal{T}_n^+(U) + \mathcal{T}_n^-(U))p_n. \quad (1)$$

Here \mathcal{T}_n^\pm are the conditional probabilities per unit time of a 1-step jump to $n \pm 1$, and $(\mathcal{T}_n^+(U) + \mathcal{T}_n^-(U))^{-1}$ is the mean waiting time at the n th site. U represents the density of the control species, and is given by

$$U = \begin{pmatrix} \vdots & \vdots & \cdots & \vdots \\ u_{1,n-1/2} & u_{2,n-1/2} & \cdots & u_{k,n-1/2} \\ u_{1,n} & u_{2,n} & \cdots & u_{k,n} \\ u_{1,n+1/2} & u_{2,n+1/2} & \cdots & u_{k,n+1/2} \\ \vdots & \vdots & \cdots & \vdots \end{pmatrix}, \quad (2)$$

for k control species. We have defined the control species on a lattice of half step size, i.e. $u_{j,n-1/2}$ is the density of species u_j at position $n - 1/2$. The three different types of models we consider here are characterized by the dependence of the transition rates on U . Following the classification of [29], we define these as *strictly local*, *barrier* and *gradient* models.

2.1. Strictly Local Models

In this model the probability of a jump depends only on the level of control species at the site of the walker. We denote by \mathbf{u}_n the densities of control species u_1, \dots, u_k at site n . We assume that the domain Ω is homogeneous and isotropic, and therefore the transition probabilities do not depend directly on the lattice site, but only on local densities \mathbf{u}_n . It follows that $\mathcal{T}^- = \mathcal{T}^+(\equiv \mathcal{T})$, and consequently (1) becomes

$$\frac{\partial p_n}{\partial t} = \mathcal{T}(\mathbf{u}_{n-1})p_{n-1} + \mathcal{T}(\mathbf{u}_{n+1})p_{n+1} - 2\mathcal{T}(\mathbf{u}_n)p_n. \quad (3)$$

We define $x = nh$, extend the function p to R , and expand the right hand side to second order in h as a function of x . We introduce a scaling of the transition rates, $\mathcal{F}(\mathbf{u}) = \lambda \mathcal{T}(\mathbf{u})$, with the property that the limit $\lim_{h \rightarrow 0, \lambda \rightarrow \infty} \lambda h^2 =$ positive constant ($\equiv D$) exists, then in this diffusion limit,

$$\frac{\partial p}{\partial t} = D \frac{\partial^2}{\partial x^2} (\mathcal{F}(\mathbf{u}) p), \tag{4}$$

The existence of this limit depends on the existence of *a priori* bounds on higher-order derivatives. In higher space dimensions the second derivative is replaced by the Laplacian. Equation (4) is subject to initial conditions and, when a finite domain is considered, boundary conditions. Furthermore p should always be nonnegative.

In one dimension the particle flux is

$$J = -D \frac{\partial (\mathcal{F}(\mathbf{u}) p)}{\partial x} = -D (\mathcal{F}(\mathbf{u})) \frac{\partial p}{\partial x} - D p \frac{\partial (\mathcal{F}(\mathbf{u}))}{\partial x}. \tag{5}$$

We define the *chemotactic sensitivity to species i* , χ_i , by

$$\chi_i = -D \mathcal{F}_{u_i} \tag{6}$$

and then can write the flux as

$$J = -D (\mathcal{F}_i(\mathbf{u})) \frac{\partial p}{\partial x} + p \sum_{i=1}^k \chi_i(\mathbf{u}) \frac{\partial u_i}{\partial x}. \tag{7}$$

If $\chi_i > 0$ (i.e., $\mathcal{F}_{u_i} < 0$), species i is an attractant and cells move up the gradient of i at a speed that may depend on other species via the dependence of χ_i on \mathbf{u} . However the global movement is determined by the sum of the responses to the individual gradients.

2.2. Barrier models

In the *barrier model* the transition rates for a cell at site n depend on \mathbf{u} at $n \pm 1/2$. One finds that without further conditions on the transition rates there is no directed movement in response to the signal; the chemotactic sensitivity vanishes identically [29]. However, if the transition rates are renormalized so that the mean waiting time is constant across the domain, then aggregation may occur. Thus we define the *renormalized transition rates* \mathcal{N}^\pm as

$$\mathcal{N}_n^+(U) + \mathcal{N}_n^-(U) = \text{constant}, \tag{8}$$

and without loss of generality we take the constant as 1. The above equation is satisfied by choosing the following forms for our transition rates,

$$\mathcal{N}_n^\pm(U) = \mathcal{N}^\pm(\mathbf{u}_{n-1/2}, \mathbf{u}_{n+1/2}) = \frac{\mathcal{F}(\mathbf{u}_{n\pm 1/2})}{\mathcal{F}(\mathbf{u}_{n+1/2}) + \mathcal{F}(\mathbf{u}_{n-1/2})}, \tag{9}$$

where $\mathcal{N}^\pm : \mathbf{R}^k \times \mathbf{R}^k \rightarrow \mathbf{R}$. We again assume that the lattice is homogeneous, we rescale the renormalized transition rates as $\mathcal{N} = \lambda\mathcal{N}$, and we assume that $D \equiv \lim_{n \rightarrow \infty, h \rightarrow 0} \frac{\lambda h^2}{2}$ exists. Then in the diffusion limit we obtain

$$\frac{\partial p}{\partial t} = D \frac{\partial}{\partial x} \left(\frac{\partial p}{\partial x} - 2p \sum_{j=1}^k (\mathcal{N}_{1,j} - \mathcal{N}_{2,j}) \frac{\partial u_j}{\partial x} \right). \tag{10}$$

Here $\mathcal{N}_{1,j}$ represents the derivative with respect to the j^{th} component of the first argument and $\mathcal{N}_{2,j}$ represents the derivative with respect to the j^{th} component of the second argument, both evaluated at $(\mathbf{u}_n, \mathbf{u}_n)$. These are determined from Equation (9), and Equation (10) becomes

$$\frac{\partial p}{\partial t} = D \frac{\partial^2 p}{\partial x^2} - D \frac{\partial}{\partial x} \left(p \sum_{j=1}^k (\ln \mathcal{F})_{u_j} \cdot \frac{\partial u_j}{\partial x} \right). \tag{11}$$

Thus the chemotactic sensitivity with respect to species i for the renormalized barrier model is given by

$$\chi_i = D(\ln \mathcal{F})_{u_i}. \tag{12}$$

2.3. Non-local or gradient models

The non-local model is based on assumption that the transition rates depend on differences between lattice sites of the density of the control species. In the simplest case one supposes only nearest neighbor differences, and then can define $\mathcal{F}_{n\pm 1}^\mp : U \rightarrow \mathbf{R}$ by

$$\mathcal{F}_{n-1}^+ = \alpha + \beta(\tau(\mathbf{u}_n) - \tau(\mathbf{u}_{n-1})), \tag{13}$$

$$\mathcal{F}_{n+1}^- = \alpha + \beta(\tau(\mathbf{u}_n) - \tau(\mathbf{u}_{n+1})), \tag{14}$$

and $\tau : \mathbf{R}^k \rightarrow \mathbf{R}$ with $\alpha(\geq 0)$ and β constants. This gives the master equation

$$\begin{aligned} \frac{\partial p_n}{\partial t} = & \alpha(p_{n+1} - 2p_n + p_{n-1}) - \beta(\tau(\mathbf{u}_{n+1}) - \tau(\mathbf{u}_n))(p_{n+1} + p_n) \\ & - \beta(\tau(\mathbf{u}_n) - \tau(\mathbf{u}_{n-1}))(p_n + p_{n-1}). \end{aligned} \tag{15}$$

We assume a scaling in the transition rates such that $D = \lim_{h \rightarrow 0, \lambda \rightarrow \infty} \lambda h^2$, and we obtain in the diffusion limit

$$\frac{\partial p}{\partial t} = D\alpha \frac{\partial^2 p}{\partial x^2} - 2D\beta \frac{\partial}{\partial x} \left(p \sum_{i=1}^k \frac{\partial \tau}{\partial u_k} \cdot \frac{\partial u_k}{\partial x} \right). \tag{16}$$

Thus the individual tactic sensitivities are given by

$$\chi_i = 2D\beta\tau_{u_i} \tag{17}$$

and the taxis is with respect to species i is positive if $\tau_{u_i} > 0$.

3. The chemotactic sensitivities for multiple signals

It is clear from the preceding derivations that the dependence of the chemotactic sensitivities on the control species arises from the dependence of the transition rates on U . In this section we derive various chemotactic sensitivity functions and show in particular that the presence of multiple signals carries with it the possibility of competition and nonlinear interactions in any of the detection, transduction and response steps.

3.1. Linear

The simple example of linear dependence of the transition rate on \mathbf{u} , given by $\mathcal{F} = T_0 + \mathbf{b} \cdot \mathbf{u}$ where T_0 and \mathbf{b} are such that $\mathcal{F} > 0$, illustrates key differences in behavior between the three models. It follows from (6), (12) and (17) that the chemotactic sensitivities for the three models are

$$\chi_j = -Db_j, \quad \chi_j = D \frac{b_j}{T_0 + \mathbf{b} \cdot \mathbf{u}}, \quad \chi_j = 2D\beta b_j. \quad (18)$$

In the barrier model the chemotactic sensitivity is monotone decreasing in the total chemical concentration if all b_i s are positive, whereas the other models have constant sensitivity with respect to all species. The sign of the sensitivities imply that the local model results in aggregation at low concentrations of species j if $b_j > 0$, whereas barrier and gradient models lead to aggregation at high concentrations under the same condition [29].

3.2. Receptor-based response laws

The linear law used above is based on the assumption that the transition rate contains a basal rate a and a component proportional to the concentration. However signals are often detected via receptors or other detectors on the surface, and since their number is limited, the transition rate cannot increase indefinitely. Moreover, at the cellular level receptors frequently span the membrane and are inactive when free of ligand, but active when bound. In the absence of a detailed transduction scheme we assume that when there is a single control species the response is proportional to the fraction of receptors that is occupied by the control species [29]. Thus if the binding reaction is written



then the fraction of activated receptors is given by $R_a = R_0 u / (K + u)$, where $K = k^- / k_+$ and $R_0 = R_a + R_i$ is the total number of cell surface receptors. If the transition rate comprises a basal rate and a component proportional to the total number of occupied receptors, then for the local and renormalized barrier models we have that

$$\mathcal{F} = T_0 + T_1 \frac{R_0 u}{K + u} \quad (20)$$

and this leads to chemotactic sensitivities of the form

$$\chi = -D \frac{T_1 R_0 K}{(K + u)^2}$$

for strictly local sensing, and

$$\chi = D \frac{T_1 K R_0}{(K + u)[T_0(K + u) + T_1 R_0 u]}$$

for the renormalized barrier model.

Similarly, if we assume that $\tau = R_0 u / (K + u)$ for the gradient model we obtain the sensitivity

$$\chi = \frac{\chi_0}{(K + u)^2} \tag{21}$$

where $\chi_0 = 2DR_0K\beta$.

It should be noted that now the sensitivity is monotone decreasing in all cases, and does so quadratically at large u , which reflects the fact that the detection machinery saturates at large signal strengths.

3.2.1. Different receptor types

When there are two distinct signals present there are two different types of sensitivities, depending on whether the signals bind competitively to the same receptor or whether there is a different receptor for each signal. Experimental evidence suggests that both cases occur depending on the specificity of the receptors. Some receptors detect only one signal, whereas in other cases the cell surface contains several types of chemotactic receptors, each receptive to a small group of signaling chemicals (see [31] and [20]).

In the latter case, two types of chemoattractant molecules, u and v , bind to two different receptor types, R_u and R_v . This is a straightforward extension of the one species case, and we derive the following expressions for the number of activated receptors, R_{a_u} and R_{a_v} :

$$R_{a_u} = \frac{R_{0_u} u}{K_u + u}, \quad R_{a_v} = \frac{R_{0_v} v}{K_v + v}. \tag{22}$$

R_{0_u} and R_{0_v} are the total number of receptors of type R_u and R_v , respectively. $K_u = k_1^- / k_1^+$ and $K_v = k_2^- / k_2^+$, where k_1^- , k_1^+ , k_2^- and k_2^+ are the rate constants due to rate equations similar to that given by (19). It is straightforward to extend the above to n chemical species, and we obtain the following expression for the total number of activated receptors:

$$\sum R_{a_{u_j}} = \sum_{j=1}^n \frac{R_{0_{u_j}} u_j}{K_j + u_j}, \tag{23}$$

where $R_{a_{u_j}}$ is the number of activated receptors of type R_{u_j} , $R_{0_{u_j}}$ is the total number of receptors of type R_{u_j} and $K_j = k_j^- / k_j^+$. Using the above expression for

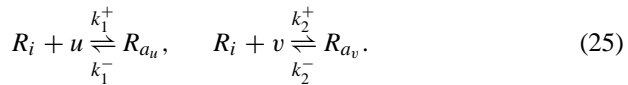
the transition rate for the gradient model we find that the individual chemotactic sensitivities are given by

$$\chi_i = \frac{2D\beta R_{0u_i} K_i}{(K_i + u_i)^2}. \tag{24}$$

It is clear from this that these sensitivities have the same form as the sensitivity in the presence of a single chemical signal, which is a result of the fact that there is no interaction of the signals at the detection stage.

3.2.2. Same receptor type

However, if the signals bind competitively then we expect to see this interaction of the signals reflected in the chemotactic sensitivities. Now we suppose that an inactive receptor R_i is activated by binding to either of two molecules, u or v . Thus the binding reactions are



and we assume that the total number of receptors $R_0 = R_{au} + R_{av} + R_i$ is constant. Assuming binding of either of the molecules occurs on the same time scale and is faster than the subsequent transduction and movement response, we have

$$[R_0 - (R_{au} + R_{av})] u k_1^+ = k_1^- R_{au}, \tag{26}$$

$$[R_0 - (R_{au} + R_{av})] v k_2^+ = k_2^- R_{av}. \tag{27}$$

If the transition rate is proportional to the number of activated receptors, $R_{au} + R_{av}$, we find from (26) and (27) that

$$R_{au} + R_{av} = \frac{R_0(k_1^+ k_2^- u + k_2^+ k_1^- v)}{k_1^- k_2^- + (k_1^+ k_2^- u + k_2^+ k_1^- v)}. \tag{28}$$

More generally, for the case of n species, u_1, \dots, u_n , we define R_{au_i} to be the number of receptors activated by chemical species u_i and R_0 to be the total number of receptors. Following the above procedure we derive

$$\sum_{i=1}^n R_{au_i} = \frac{R_0 [\sum_{i=1}^n u_i K_p / K_i]}{K_p + [\sum_{i=1}^n u_i K_p / K_i]}, \tag{29}$$

where $K_j = k_j^- / k_j^+$ and $K_p = \prod_{j=1}^n K_j$.

With the above expression for the transition rate, we find that for a gradient model the chemotactic sensitivity for the j^{th} species is given by

$$\chi_j = \frac{2D\beta K_p K_j}{(K_p + [\sum_{i=1}^n u_i K_p / K_i])^2}. \tag{30}$$

The only variation in the sensitivity for each individual species results from the different values of K_j .

It follows that the total chemotactic flux is given by

$$\frac{2D\beta p}{(K_p + [\sum_{i=1}^n u_i K_p / K_i])^2} \sum_j K_p K_j \nabla u_j, \quad (31)$$

and the direction of the flux is determined by a linear function of the individual chemical gradients.

3.2.3. Nonlinear interaction sensitivity laws

Thus far the transition rates are simply assumed to be a linear combination of the total number of activated receptors, which means that are a number of independent signaling pathways whose outputs are additive. However, there may also be parallel pathways, both of which must be activated to induce movement. Thus we assume a dependence based on the product of the activated fraction of receptors, which gives

$$\mathcal{F} = \frac{R_{0,u}u}{(K_u + u)} \frac{R_{0,v}v}{(K_v + v)}. \quad (32)$$

The chemotactic sensitivities for the gradient model are therefore given by

$$\chi_u = \frac{\chi_{0,u}v}{(K_u + u)^2(K_v + v)}, \quad \chi_v = \frac{\chi_{0,v}u}{(K_v + v)^2(K_u + u)}. \quad (33)$$

where $\chi_{0,u} \equiv 2D\beta K_u R_{0,u} R_{0,v}$ and $\chi_{0,v} \equiv 2D\beta K_v R_{0,v} R_{0,u}$. Notice that the above implies that for low v the chemotactic sensitivity response to species u is much weaker than the response at high concentrations of v . Thus, by reducing the level of v the chemotactic response of the cell may be drastically reduced despite the presence of gradients of u . This introduces another level of control, if for example, the production of the signaling chemicals depends on the cell density.

4. Spatial response to multiple cues

The patterns of the spatial distribution of a cell population responding to multiple cues is illustrated in the following theoretical model. We consider a Turing system [39] as a mechanism for providing spatially heterogeneous chemical distributions to which a cell population chemotactically responds. More formally, a cell population density, $n(\mathbf{x}, t)$, is defined on the spatial domain $\Omega \in \mathbf{R}^n$. Chemicals u and v , which are called morphogens, evolve according to a system of reaction-diffusion equations. The cell population responds chemotactically to both chemical species, leading to the equations

$$\frac{\partial n}{\partial t} = \nabla \cdot \{D_n \nabla n - n \chi_1(u, v) \nabla u - n \chi_2(u, v) \nabla v\}, \quad (34)$$

$$\frac{\partial u}{\partial t} = \nabla \cdot (D_u \cdot \nabla u) + f(u, v), \quad (35)$$

$$\frac{\partial v}{\partial t} = \nabla \cdot (D_v \cdot \nabla v) + g(u, v), \quad (36)$$

where χ_1 and χ_2 are the chemotactic sensitivity functions and f and g define the chemical kinetics. Herein cell and chemical diffusion coefficients, D_n , D_u and D_v , are taken as constant. In this first model we assume that the evolution of the morphogens is independent of the cell density. We will refer to the above equations as the *hybrid* model.

We first consider a uniformly distributed cell population and, without loss of generality, set $n(\mathbf{x}, 0) = 1$. Initial conditions for the chemical concentrations are taken as small random perturbations about the homogeneous steady state. Boundary conditions are taken to be zero flux. The application of the boundary conditions with the zero population kinetics imposes a conservation law on total cell population, *viz.*

$$\int_{\Omega} n(\mathbf{x}, t) d\mathbf{x} = \int_{\Omega} n(\mathbf{x}, 0) d\mathbf{x}. \tag{37}$$

We assume that the equations (34)–(36) have a single positive homogeneous steady state (n_0, u_0, v_0) , where without loss of generality we take $n_0 = 1$. It is also assumed that the structure of f and g is such that (35) and (36) have a stable nonconstant steady state solution (a Turing pattern) for suitable choices of the kinetic parameters, and that the uniform steady state is unstable to small perturbations.

4.1. Patterning in one dimension

We first consider the one-dimensional domain, $\Omega = [0, L]$, and suppose that the kinetics are described by a simplified model for the glycolysis reaction [27, 9]. The model (34)–(36) is then given by

$$\frac{\partial n}{\partial t} = \frac{\partial}{\partial x} \left[D_n \frac{\partial n}{\partial x} - n\chi_1(u) \frac{\partial u}{\partial x} - n\chi_v(v) \frac{\partial v}{\partial x} \right], \tag{38}$$

$$\frac{\partial u}{\partial t} = D_u \frac{\partial^2 u}{\partial x^2} + \delta - \kappa u - uv^2, \tag{39}$$

$$\frac{\partial v}{\partial t} = D_v \frac{\partial^2 v}{\partial x^2} + \kappa u + uv^2 - v, \tag{40}$$

with zero-flux boundary conditions:

$$D_n \frac{\partial n}{\partial x} - n\chi_1(u) \frac{\partial u}{\partial x} - n\chi_v(v) \frac{\partial v}{\partial x} = 0 \tag{41}$$

$$\frac{\partial u}{\partial x} = \frac{\partial v}{\partial x} = 0 \tag{42}$$

at $x = 0$ and $x = L$. Thus all three components satisfy a homogeneous Neumann boundary condition.

The absence of cellular feedback results in a decoupling of the cell movement equation from the reaction-diffusion system. Thus, temporarily we ignore the cell equation (38) and focus on evolution of pattern in the reaction-diffusion model. A linear analysis of Equations (39)–(40) about the homogeneous steady state, $(u_0, v_0) = (\delta/(\kappa + \delta^2), \delta)$, gives a prediction for initial pattern evolution

and the parameter region wherein Turing instabilities can develop. It does not provide a specific analytical prediction of the pattern at the heterogeneous steady state because, as the solution grows, nonlinear terms become dominant and the linear analysis is no longer valid. An analytical approximation for the time independent solutions to Equations (39)–(40) can be obtained, and the results are summarized in the Appendix. The general approach can be found in a number of texts [13, 16]. To first order in the deviation from the uniform steady state, the spatial distribution of the morphogens is given by

$$u(x) = u_0 + u_1 \cos jx, \quad (43)$$

$$v(x) = v_0 + v_1 \cos jx, \quad (44)$$

where u_1 and v_1 can be determined explicitly for a particular set of parameters through the asymptotic expansion. In Figure 1 (a) we compare analytical and numerical approximations for the concentrations of u and v , using the parameters of the figure caption. The validity of solutions derived from a bifurcation analysis, given by Equations (43)–(44), is demonstrated by the very close correspondence with the numerically derived concentrations.

When the chemotactic sensitivities are non-zero it is possible that patterning of the cell population via the response to the nonuniform distribution of the morphogens, given (43)–(44). The steady state cell distribution that satisfies the boundary conditions is given by

$$n(x) = K \exp \left(\int_0^x \frac{1}{D_n} \left(\chi_1 \frac{du}{dx} + \chi_2 \frac{dv}{dx} \right) dx \right), \quad (45)$$

where the constant K can be evaluated using the conservation equation (37), once the u and v distributions are known.

One of the primary characteristics of a spatial pattern of the cell population (or chemical species) is the number of maxima and minima. For chemical patterns that arise via a Turing instability (with zero flux boundary conditions and close to the bifurcation point), this is relatively straightforward: the pattern possesses a common wavelength with equally spaced peaks. Moreover, the spatial location of turning points is the same for both chemical species – they are either in phase (for pure activator-inhibitor kinetics) or in antiphase (for cross activator-inhibitor kinetics) [9]. The glycolysis reaction is an example of a cross activator-inhibitor reaction system: peaks of u occur at troughs of v and *vice versa*.

4.1.1. Patterning in response to a single cue

The effect of taxis on cell patterning can be evaluated by a comparison between the critical points of the cell density and the critical points in the chemical concentrations. The response to one chemical is considered by taking $\chi_2 = 0$ in Equation (45) and assuming that χ_1 is a function of u only. We determine

$$\frac{dn}{dx} = \frac{K}{D_n} \exp \left(\frac{1}{D_n} \int \chi_1(u) \frac{du}{dx} dx \right) \chi_1 \frac{du}{dx}. \quad (46)$$

Thus, providing χ_1 is non-zero and continuous for all $u(x) > 0$, the turning points in the cell density coincide with the turning points in the chemical distribution, since $K \exp\left(\frac{1}{D_n} \int \chi_1(u) \frac{du}{dx} dx\right)$ is positive. All standard response laws, i.e. constant, logistic and receptor, satisfy these conditions, although one can construct a *biphasic* form that does not fall into this category.

We suppose that the chemical u binds to two different cell surface receptors R and S . The fraction of occupied receptors of each type will be given by $R_0u/(k_1+u)$ and $S_0u/(k_2+u)$ respectively. We further assume that activation of R receptors induces an attractive response, while activation of S receptors induces a repulsive response. Then if the transition rate is a linear combination of the activated receptors we have that

$$\mathcal{F}(u) = T_0 + \frac{T_1 R_0 u}{k_1 + u} - \frac{T_2 S_0 u}{k_2 + u}. \quad (47)$$

We set $\alpha = T_1 R_0$ and choose $k_1 = 1$ and $T_2 S_0 = 1$ for convenience. One finds that the chemotactic sensitivity (using a gradient-based transition rule) is

$$\chi_1(u) = \frac{\alpha k_2^2 - 1 + 2u(\alpha k_2 - 1) + u^2(\alpha - 1)}{(1 + u)^2(k_2 + u)^2}. \quad (48)$$

If we set $\alpha < 1$ and $\alpha k^2 > 1$, then in addition to turning points that coincide with those of the chemical concentration, there additional critical points corresponding to locations at which χ_1 changes sign. This *biphasic* law models chemotactic attraction at lower chemical concentrations, and chemotactic repulsion at higher concentrations. Consequently, cells aggregate at an intermediate level of concentration. In response to the guidance cue BDNF (brain-derived neurotrophic factor), nerve growth cones have been shown to display both chemoattraction and chemorepulsion, depending on the level of cAMP [35].

4.1.2. Cell patterning in response to both chemicals

If we specify that the chemotactic sensitivities are constants $\chi_1 = \alpha$ and $\chi_2 = \beta$, then the solution for cell density at a heterogeneous steady state can be obtained analytically, and one finds that

$$n(x) = K_c \exp\left(\frac{\alpha u + \beta v}{D_n}\right), \quad (49)$$

where K_c is a constant. Thus the spatial distribution of the cell density is determined by the linear combination $\alpha u + \beta v$ of the morphogens. In Figure 1 (b)–(d) we plot the function $\alpha u + \beta v$ for constant β and increasing α , using the analytically- and numerically-computed u and v shown in Figure 1(a). If α is sufficiently different from $-\beta v_1/u_1$, there is little difference between the numerically- and analytically-derived values of $\alpha u + \beta v$, as seen in Figure 1(b). However, as α is increased the structure of the analytically- and numerically-computed profiles diverges, as in (c), and for a small range of α near $-\beta v_1/u_1$ the numerical solution displays greater

structure, with two peaks in the density (cf. (d)). Although the patterns show very different *structure*, the maximum difference between the two profiles for all α, β is always of the order ϵ^2 , where a definition for ϵ can be found in the appendix. This arises from the fact that the difference between the numerical and analytical approximations of the chemical concentrations is of order ϵ^2 . As α is increased above $-\beta v_1/u_1$ the two profiles again display the same structure.

These results suggest that the analytical approximation for $n(x)$ is only valid outside a neighborhood of the line $\alpha = -\beta v_1/u_1$. This restriction can be understood by examining the second order terms in the asymptotic expansion for the chemical concentration done in the Appendix. The second order approximations

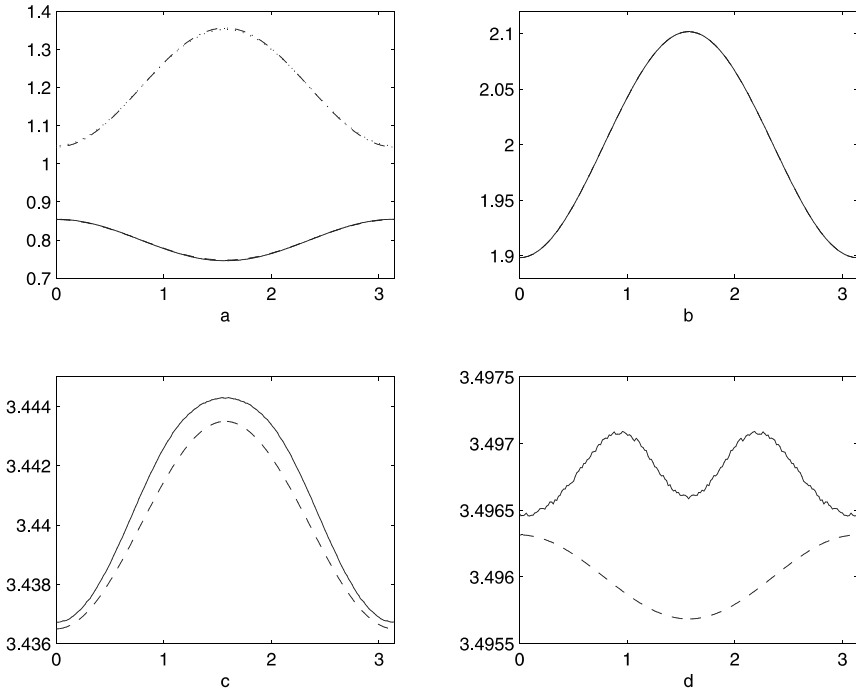


Fig. 1. (a) Comparison between analytical and numerically derived chemical concentrations. u numerical (solid) and analytical (dashed), v numerical (dot-dash) and analytical (dotted). The discrepancy is very small, reflected by these lines overlying one another. (b) – (d) Comparison between $\alpha u + \beta v$ using the analytical and numerical solutions for u and v plotted in (a). This function reflects the form of the cell density at steady state under constant sensitivity rules. (b) $\alpha/D_n = \beta/D_n = 1.0$, (c) $\alpha/D_n = 2.8$ and $\beta/D_n = 1.0$, (d) $\alpha/D_n = 2.87$ and $\beta/D_n = 1.0$. For the majority of $\alpha/D_n - \beta/D_n$ space the two predictions match. For example, in (b) the solutions lie on each other and are difficult to discern. As α/D_n is increased towards $-\beta v_1/D_n u_1$, the two forms diverge, (see (c)) until they have different structure, (see (d)). Simulations use $\delta = 1.2, \kappa = 0.06, L = \pi, D_u = 1.0$ and $D_v = 0.09809$. The analytical forms, as determined by the Appendix, use $u_0 = 0.8, v_0 = 1.2, u_1 = 0.0545, v_1 = -0.1561$

of the chemical concentrations are given by functions of the form

$$u(x) = u_0 + u_1\epsilon \cos jx + \epsilon^2 (u_{20} + u_{21} \cos jx + u_{22} \cos 2jx) \quad (50)$$

$$v(x) = v_0 + v_1\epsilon \cos jx + \epsilon^2 (v_{20} + v_{21} \cos jx + v_{22} \cos 2jx). \quad (51)$$

From the expansion in the Appendix, we only know the magnitudes of $u_0, u_1, u_{20}, u_{22}, v_0, v_1, v_{20}$ and v_{22} . The bifurcation analysis does not determine the magnitudes of u_{21} and v_{21} , but does determine the *ratio*, which is given by $u_{21}/v_{21} = u_1/v_1$.

For the above forms, the critical points in cell density are the solutions to the equation

$$\epsilon j(\alpha u_1 + \beta v_1 + \epsilon(\alpha u_{21} + \beta v_{21})) \sin jx + 2j\epsilon^2(\alpha u_{22} + \beta v_{22}) \sin 2jx = 0, \quad (52)$$

which, in turn, has solutions

$$\sin jx = 0, \quad (53)$$

$$4\epsilon(\alpha u_{22} + \beta v_{22}) \cos jx = -(\alpha u_1 + \beta v_1 + \epsilon(\alpha u_{21} + \beta v_{21})). \quad (54)$$

The former defines the same primary turning points as for the first order approximations, which correspond with those of the chemical concentrations. The latter only has solutions if $\alpha u_1 + \beta v_1 = \mathcal{O}(\epsilon)$, and therefore we choose chemotactic coefficients such that $\alpha u_1 + \beta v_1 = 0$. From the analysis in the appendix we have $\alpha u_{21} + \beta v_{21} = 0$, and thus if $\alpha u_{22} + \beta v_{22} \neq 0$, Equation (54) predicts additional critical points that are out of phase with the primary critical points. For the parameters considered here, this assumption above is valid. If we fix $\beta > 0$ and increase α from below the line $-v_1\beta/u_1$, the cell density profiles change nature from a form equivalent to the chemical profiles to one with a greater number of turning points, and the latter arise as the result of the superposition of $\cos jx$ and $\cos 2jx$ waves. Hereafter we label such cell patterns as *complex* to distinguish them from the simple patterns in which the critical points coincide with those of the chemical concentration.

The validity of the above analysis is strengthened by a comparison of analytical and numerical solutions for the special case, $\alpha = -v_1\beta/u_1$. We use this solution to obtain an analytical determination of the amplitude of the cell density for the $\cos 2jx$ wave type pattern, as all $\cos jx$ terms drop out (at least up to second order),

$$n(x) = K \exp \left(\frac{(\alpha u_0 + \beta v_0 + \epsilon^2 \alpha u_{20}) + \epsilon^2 (\alpha u_{22} + \beta v_{22}) \cos 2jx}{D_n} \right). \quad (55)$$

When this is evaluated for the parameters of Figure 1 with $\alpha/D_n = 5.5$ and $\beta/D_n = 1.92$, we obtain an amplitude of 0.00046, which compares favorably with the amplitude of the pattern derived via numerical simulation, 0.00048. The discrepancy is $\mathcal{O}(\epsilon^3)$, where a definition for ϵ can be found in the Appendix. Thus cells may exhibit density patterns of greater spatial complexity than that of the underlying chemical concentration profiles in response to multiple chemotactic cues.

Next we compare these results with those obtained using sensitivities of the form

$$\chi_1 = \frac{\alpha}{(k_1 + u)^2}, \quad \chi_2 = \frac{\beta}{(k_2 + v)^2}, \tag{56}$$

where α, β, k_1 and k_2 are constants and $k_1, k_2 > 0$. In this case, the form of the cell density at the heterogeneous steady state can be found as

$$n(x) = K_r \exp\left(-\frac{1}{D_n} \left(\frac{\alpha}{k_1 + u(x)} + \frac{\beta}{k_2 + v(x)}\right)\right). \tag{57}$$

where K_r is a constant. A calculation of the locations of non-trivial turning points gives the following solutions,

$$\alpha u_1 (v_0 + k_2 + v_1 y)^2 + \beta v_1 (u_0 + k_1 + u_1 y)^2 = 0, \tag{58}$$

where $y = \cos jx$. Rearranging this expression gives the following solutions for y ,

$$y_{\mp} = \frac{\pm(v_0 + k_2)\sqrt{\frac{-\alpha u_1}{\beta v_1}} - u_0 + k_1}{u_1 \mp v_1 \sqrt{\frac{-\alpha u_1}{\beta v_1}}}. \tag{59}$$

Of course the only real solutions lie in the range $[-1, 1]$, and it is easy to verify that either there is no solution or one solution that satisfies this criterion, depending on the parameters. When one solution does lie in this range we predict that complex patterns develop. These predictions are confirmed by a comparison of numerical and analytical results. Examples of complex patterns are shown in Figure 2. While similar to those observed for constant laws, these patterns have greater amplitude and occur for a larger range of parameters.

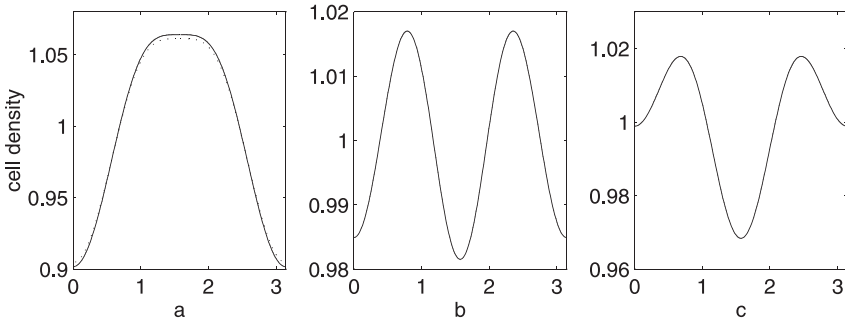


Fig. 2. Patterns predicted by the model with receptor response laws given by (56). We use the analytical predictions determined in the Appendix for the parameters given in Figure 1 ($u_0 = 0.8, v_0 = 1.2, u_1 = 0.0545, v_1 = -0.1562$). Figures (a) through (c) demonstrate increasing complexity as we move through α - β space. Notice that the amplitude of the complex patterns is larger than corresponding patterns (Figure 1) that arise for constant sensitivity laws

4.2. Patterning in two dimensions

In two dimensions, we assume chemical concentrations of the form,

$$u(x, y) = u_0 + u_1 \cos\left(\frac{n\pi x}{L_x}\right) \cos\left(\frac{m\pi y}{L_y}\right), \quad (60)$$

$$v(x, y) = v_0 + v_1 \cos\left(\frac{n\pi x}{L_x}\right) \cos\left(\frac{m\pi y}{L_y}\right). \quad (61)$$

For the above forms two elementary pattern types exist: If n and m are non-zero, we have a checkerboard type pattern composed of peaks and troughs, namely *spots*, whereas if only one of n or m is non-zero then the pattern consists of *stripes*.

Using the receptor law sensitivities, it is straightforward to analytically demonstrate that the one-dimensional results carry over to two dimensions. The types of complex patterns formed in the cell density can be classified as (1) rings, (2) interspersing large and small spots and (3), interspersed broad and narrow stripes. Figure 3 illustrates these pattern types.

We now consider more complicated chemotactic sensitivity laws. Extending the derivation of the biphasic sensitivity law earlier to two chemical species, we assume a transitional response,

$$\mathcal{T}(u) = T_0 + \frac{T_1 R_1 u}{k_1 + u} - \frac{T_2 R_2 u}{k_2 + u} + \frac{T_3 R_3 v}{k_3 + v} - \frac{T_4 R_4 u}{k_4 + u}. \quad (62)$$

For this transitional response, the chemotactic sensitivities terms χ_1 and χ_2 take the form given by Equation 48. Analytical results under these laws give rise to more complicated patterns than for the “standard” laws considered earlier. In two dimensions, we observe patterns such as the spots inside rings or variant stripes, as shown in Figure 4.

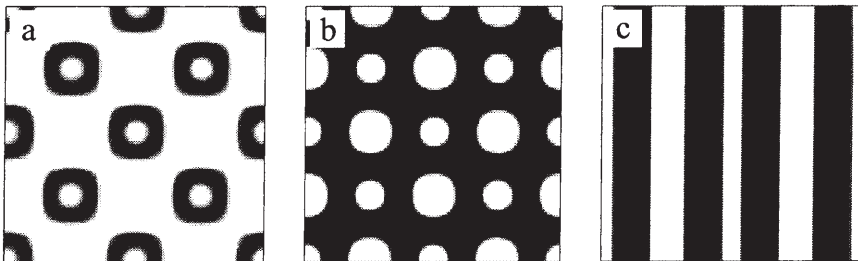


Fig. 3. Typical examples of the complex patterns observed in two dimensions. (a) Rings (b) Interspersed large and small spots and (c) Alternating broad and narrow stripes. Patterns obtained using receptor type laws for underlying chemical patterns such that $u_0 = 0.8$, $v_0 = 1.2$, $u_1 = 0.2$ and $v_1 = -0.6$. We take $\beta/D_n = 1.0$, $k_1 = 0.8$, $k_2 = 1.0$ and $\alpha/D_n =$ (a) 2.5, (b) 1.8, (c) 1.8. A threshold has been chosen for clarity of presentation

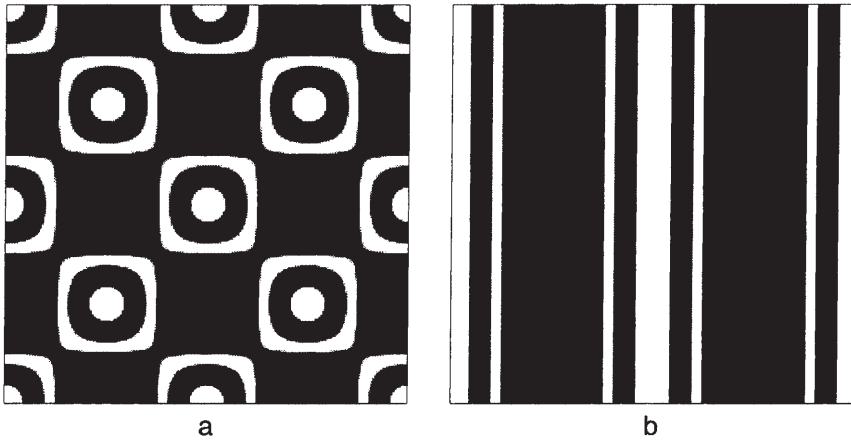


Fig. 4. Typical examples of patterns obtained under more complicated sensitivity responses. (a) Spots inside rings and (b) Series of stripes. In both simulations, we use the parameters $T_1R_1 = 1.0$, $T_2R_2 = 3.85$, $T_3R_3 = 1.0$, $T_4R_4 = 3.85$, $k_1 = 0.5$, $k_2 = 2.0$, $k_3 = 0.5$, $k_4 = 1.95$, $u_0 = v_0 = 1.0$, $u_1 = +0.5$, $v_1 = -0.3$. Once again we have chosen a threshold in the cell density to demonstrate the pattern more clearly. For (a) we use an underlying spotted chemical pattern, whereas (b) uses an underlying striped pattern

4.3. Robustness of patterns

As we have shown, when the chemotactic sensitivity depends on two chemicals each of the different types of sensitivity laws examined leads to increased complexity of the spatial distribution of the cells. For constant chemotactic sensitivities this complexity is dependent on the fine structure of the chemical distributions (which analytically corresponds to the higher order terms of the asymptotic expansions), whereas with receptor laws it arises through nonlinear terms in the sensitivity function. This fundamental difference may lead us to expect differences with respect to robustness of the patterns, and hence the applicability of different mechanisms to biological pattern formation. Robustness here refers to pattern characteristics such as amplitude of the patterns and the parameter region in which they occur. For constant sensitivity laws the amplitude of the patterns is very small, and they occur in a very restricted range of parameter space. However receptor laws produce larger amplitude pattern and these patterns exist in a larger region of parameter space.

These results are significant when the underlying chemical concentrations are less regular. For kinetic parameters that lie in a small neighborhood of the point at which the Turing instability occurs in the chemical system the pattern is very regular since the power spectrum of the solution is dominated by the amplitude of the unstable mode. However, the pattern may be much less regular far from the primary bifurcation points.

In Figure 5 (a)–(c) we display the chemical concentrations derived by numerical simulation of the two dimensional reaction-diffusion system. The patterns illustrate the two pattern types commonly observed in Turing systems: A hexagonal array ((a) and (b)) and stripes (c). Increasing the domain size in (a)–(b) results in less regular

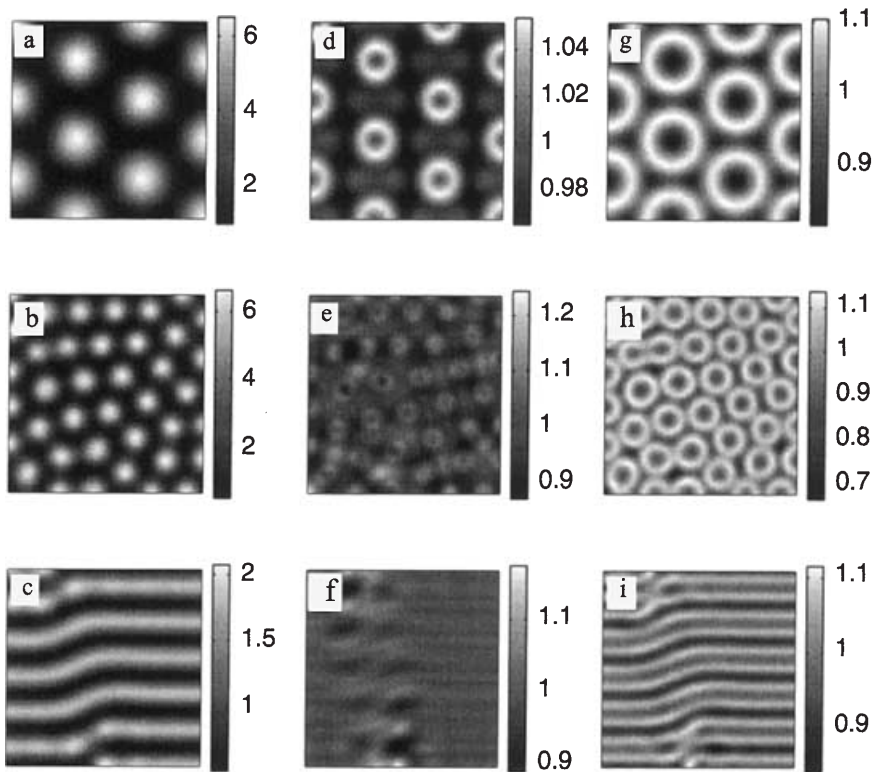


Fig. 5. Cell patterning under chemical concentrations obtained by numerical simulation of the Turing system. Left column shows heterogeneous steady state chemical patterns (v species) (a) Hexagons, $\delta 8qwe = 2.8, \kappa = 0.06, D_u = 1.0, D_v = 0.0125$, domain $[0, \pi] \times [0, \pi]$. (b) For the larger domain $[0, 2\pi] \times [0, 2\pi]$, the hexagonal patterns show less regularity. (c) Stripe solutions for parameter values $\delta = 1.2, \kappa = 0.06, D_u = 1.0, D_v = 0.08$, domain $[0, 5\pi] \times [0, 5\pi]$. Cell patterning under constant and receptor sensitivities are shown in the middle and right columns respectively. With the regular chemical concentrations (a), both constant and receptor laws can demonstrate ring type patterns, however those obtained for receptor law have a larger diameter and greater amplitude. Under less regular patterns such as the hexagons of (b) and the stripes (c), receptor laws can give clearly defined rings or thick and thin stripes, whereas no coherent pattern emerges under the constant laws

patterning. The middle and right columns show the complex patterns produced in the cell density for constant and receptor sensitivity laws, respectively. Constant laws (d) produce rings of small circumference and amplitude. Receptor laws (g), however, produce large rings of large amplitudes. Furthermore, the region of $\alpha - \beta$ parameter space over which these patterns are observed is much greater in the latter case than in the former. This aspect is critical for the production of such patterns on a large domain. A comparison of the last two columns shows that distinct rings of large amplitude (h) or alternating broad and narrow stripes (i) are obtained with receptor laws, whereas no coherent pattern occurs for the constant sensitivity laws, (e) and (f). Thus non-constant sensitivities lead to more accurate tracking of the underlying morphogen distribution.

5. Applications

5.1. Animal skin patterns

A theoretical application of the Turing model is that of Murray ([23], [24], [25]), (see also [2] and [40]), who considered a reaction-diffusion system as the underlying mechanism for pigment patterns on mammalian coats. A reaction-diffusion system establishes an underlying nonhomogeneous morphogen field which provides the information for pigment cells to differentiate into a particular type depending on the local morphogen concentration. This theory of pigmentation is attractive due to the similarity between patterns generated by the model and coat markings, but even a cursory glance through an encyclopedia of animal patterns yields exceptions. These include alternating *thick and thin stripes*, which most notably occur in species of fish (e.g. the lionfish) or reptiles (for example, the tail of the gila monster), *rings*, which are commonly observed on species of wild cat such as the jaguar, leopard and ocelot. More complex patterns include those shown by the thirteen lined ground squirrel which display stripes interspersed with a line of spots.

5.1.1. Animal markings through the hybrid model

We can apply the complex patterns exhibited by the hybrid model in the context of animal coat markings. Essentially, we propose a mechanism whereby pigment cells organize themselves spatially via a chemotactic movement response to gradients of chemicals in the reaction-diffusion system. Further differentiation into a specific pigment type may then arise through sensing a threshold of local cell density. Biological evidence suggests that the mechanism under which pigment cell precursors migrate to dermal layers of the skin may be chemotactic ([10], [18], [21], [17]) and it is not an unreasonable supposition to assume organisation of cells in the skin also occurs through chemotaxis.

In Figure 6, we compare patterns observed with the hybrid model with patterns seen on animal coats. Ring patterns obtained by numerical simulation of the model are compared with those on the jaguar, and broad and narrow stripes predicted by the model are compared with the lionfish. Theoretically, a third type of common complex pattern was obtained in two-dimensions; the large and small spots shown in Figure 3(b). Both rings and broad and narrow stripes can be observed in large regions of parameter space (under receptor sensitivity laws), and are relatively insensitive to the regularity of the underlying chemical kinetics – see section on robustness above. The large and small spots, however show much greater sensitivity to the underlying pattern. Despite the appearance of such patterns in theory or under highly regular chemical concentrations (such as in Figure 3(b)), they are less likely to arise in biological systems, where greater variation is to be expected. Intriguingly, this may be reflected in pigmentation markings. Both rings and broad/narrow stripes have been observed on the skins of a variety of animals, yet we have been unable to find biological examples of the third type.

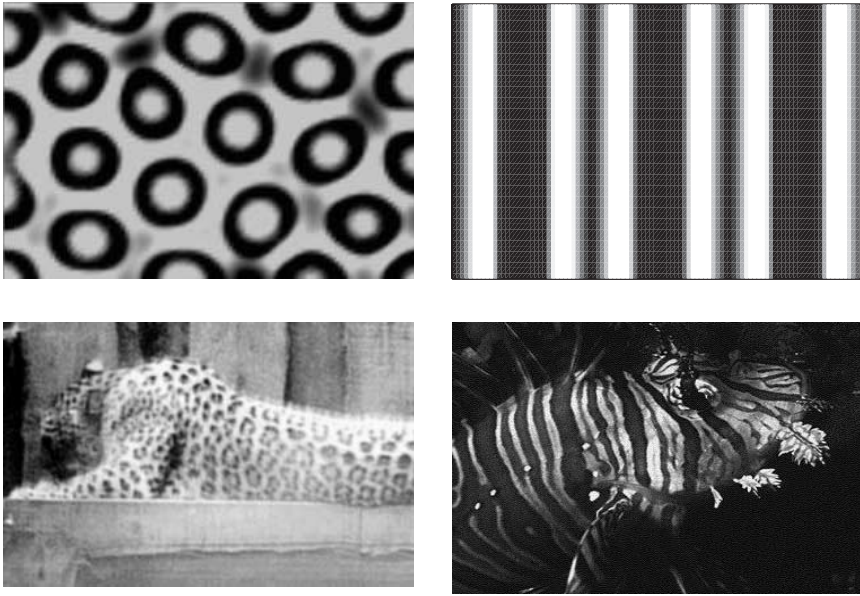


Fig. 6. Comparison between complicated animal skin patterns and patterns produced by the hybrid model. The right column compares thick and thin dark stripes with the pigmentation patterns seen on the lionfish. The left column compares ring patterns with those of the young jaguar. The lionfish picture appears by courtesy of Steve Hogan (<http://www.diversionoz.com/Steve/>)

5.2. Bacterial chemotaxis

We now consider a simple model for pattern formation in bacteria (for example, *E. coli*) in an environment containing two chemotactic substances. A detailed model for signal transduction of a single attractant at the individual cell level has been analyzed [36], but here we use a simpler continuum description that uses the receptor-based schemes developed earlier. This model illustrates how differences in the local movement rules with two species leads to significantly different macroscopic patterning. In one dimension, the cell density evolves according to the equation,

$$\frac{\partial n}{\partial t} = D_n \frac{\partial^2 n}{\partial x^2} - \frac{\partial}{\partial x} \left(n \chi_1(u, v) \frac{\partial u}{\partial x} \right) - \frac{\partial}{\partial x} \left(n \chi_2(u, v) \frac{\partial v}{\partial x} \right) \quad (63)$$

Experimentally, techniques have been developed which allow the creation of stationary linear chemical gradients in chemotaxis chambers, [14]. Consequently we shall assume stationary chemical profiles of this type in the above model. The chemotactic sensitivity functions considered are derived using transitional rates of the types considered in Section 3, summarized here in Table 1. We choose $\alpha = \beta = 10.0$, $D_n = 1.0$, $k_1 = k_2 = k_3 = 1.0$. We assume an initially homogeneous cell distribution, with no net flux of cells across the boundary. The

Table 1. Classification and functional form of the chemotactic sensitivities for the simulations

Sensitivity type	χ_1	χ_2	Classification
Same receptor	$\alpha/(k_1 + k_2u + k_3v)^2$	$\beta/(k_1 + k_2u + k_3v)^2$	Type 1
Different receptor (linear)	$\alpha/(k_1 + u)^2$	$\beta/(k_2 + v)^2$	Type 2
Different receptor (nonlinear)	$\alpha v/(k_1 + u)^2(k_2 + v)$	$\beta u/(k_2 + v)^2(k_1 + u)$	Type 3

time-independent version of this equation can be solved analytically to obtain the heterogeneous steady state.

5.2.1. Competing attractant gradients

Chemoattractant gradients of u and v are plotted in Figure 7 (left). Here we assume competing linear attractant concentrations of equal slope and maxima. The cell density at the heterogeneous steady state under the sensitivities of Table 1 in response to these attractant gradients are shown in Figure 7 (right). When both attractants are assumed to bind to the same surface receptor (Type 1), the chemotactic fluxes balance, resulting in a homogeneous cell density (solid line, Figure 7 (c)). For attractants binding to different cell surface receptors (Type 2 and Type 3), however, cell density peaks emerge at a point between the maxima of the two chemoattractants (Figure 7 (a) = linear, Figure 7 (b) = nonlinear). The saturation of response at higher chemical concentrations results in a weaker chemotactic effect at these regions, and cells aggregate in the centre.

By varying the maximum concentration (and hence slope) of v , we observe further differences in the macroscopic cell density for the various sensitivity types. In Figure 8, (a), we plot u (solid) and v (dashed) concentrations and now consider varying the maximum of v , V_m . Cell densities under Type 1 sensitivities are plotted in Figure 8 (b). With $V_m < 1.0$, the gradient of u is larger and u dominates cell movement. Consequently, cell aggregations occur at maxima of u . As V_m is increased above 1.0, however, the gradient in v is stronger, resulting in switching the cell aggregation to v maximum. A similar effect is observed for Type 2 sensi-

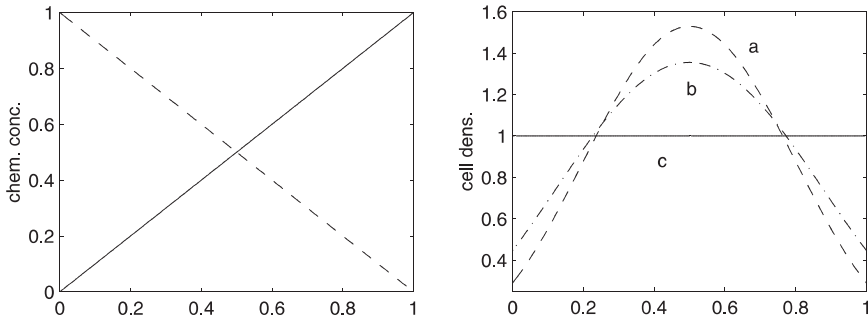


Fig. 7. Cell density response to competing attractant signals. Left: Chemical concentrations of u , solid line, and v , dashed line. Right: heterogeneous cell densities in response to these signals for (a) Type 2 sensitivities, (b) Type 3 sensitivities and (c) Type 1 sensitivities

Table 2. Table summarising the results for the bacterial cell model. Results classified in terms of the position of the aggregation with respect to the high concentrations of u or v . Note that “at u ” may mean the the aggregation is *biased* towards the higher concentrations of u , rather than at the maximum. Where the aggregation response is particularly small, we have indicated this. Summaries in bold face demonstrate where the behaviour is particularly different for one sensitivity law, as compared with the others

Sensitivity Type	Equiv. attractants		Comp. attract: various V_m		Gradient vs constant	
	Aggregation	Agg. V_m high	Agg. V_m low	Agg. V_m high	Agg. V_m low	Agg. V_m low
Type 1	None	Agg. at v	Agg. at u	Small agg. at u	Agg. at u	Agg. at u
Type 2	Centre	Agg. at v	Agg. at u	Agg. at u	Agg. at u	Agg. at u
Type 3	Centre	Agg. at u	Small agg. at v	Agg. at u	Small agg. at u	Small agg. at u

tivities, Figure 8 (c), yet in a region around $V_m = 1.0$, the cell density maximum lies between the peaks in chemical concentration. A completely different behavior occurs under Type 3 sensitivity functions, Figure 8 (d). Low values of V_m (e.g., 0.1) decrease the effective response both to u and v . Consequently, a small aggregation occurs which is biased towards the maximum concentration of v . This may initially appear counterintuitive, however from Table 1 we see that for Type 2 sensitivities and v small, χ_1 is small. A reverse effect is observed at larger values of V_m , e.g. 5.0, and the aggregation is shifted towards the u maximum. Here, a shallow gradient can be detected by the cells, despite the presence of a much stronger second signal.

5.2.2. Attractant gradient vs constant attractant level

We study the response to a single attractant gradient, yet with a uniform concentration of a second attractant. The forms for the concentrations of u (solid) and v (dashed) are plotted in Figure 9 (a), and once again we examine responses to the three sensitivity laws under variation of V_m . At high concentration levels of v and Type 1 sensitivities, cell aggregations at the u maximum is minimal, Figure 9 (b). This occurs via high levels of v resulting in occupancy of the receptors which saturates the response. Decreasing V_m results in an enhanced aggregation. For Type 2 sensitivities, the aggregation to v is the same, regardless of the level of V_m , Figure 9 (c). The opposite behaviour to that described for Type 1 sensitivities occurs under Type 3 sensitivity rules. Here, the aggregation in response to u is minimised at very low levels of V_m , and maximised at high levels, Figure 9 (d).

5.2.3. Summary of the bacteria response

The aggregation in response to two gradients demonstrates highly different behaviour, depending on the choice of sensitivity functions. These differences are summarised in Table 2. Experimental techniques which allow the creation of linear attractant gradients in chemotaxis gradients may be used to test the effect of two attractant cues, and subsequently test which sensitivity functions may apply in real

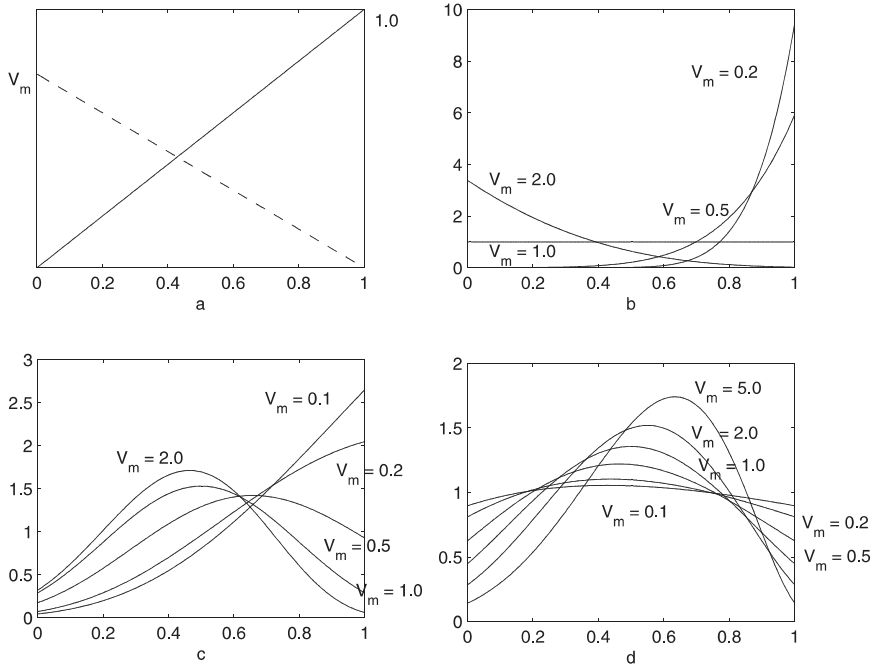


Fig. 8. Cell density response to competing attractant signals. (a) Chemical concentrations for u , solid line, and v dashed line, maximum concentration of v determined by V_m . (a) Cell densities under Type 1 sensitivities, (c) cell densities under Type 2 sensitivities, (d) cell densities under Type 3 sensitivities

systems. Type 3 sensitivities assume that the transduction from external signal to internal cell movement occurs via some nonlinear combination of the two attractant cues. The response to v for these sensitivity laws demonstrates how cells can respond to very low levels of a specific signal, despite the presence of stronger signals from other sources.

6. Discussion

In this paper we developed a model for the response of a cell population to two distinct chemicals, either of which may be an attractant or repellant, and we analyzed some of the properties of this model. We generalized the Othmer-Stevens approach [29] by modeling the tactic response to multiple signals and considered, in turn, strictly local, barrier, and gradient models. We also considered several different types of chemotactic sensitivity laws, and demonstrated that when organisms can respond to more than one chemical cue, the integration of signals via different combinations of receptor based-response laws leads to many new behavioral responses. We have shown that one manifestation of this more complex response is more complicated spatial patterns.

For instance, the model can exhibit spatial pattern of thick and thin stripes as was shown earlier in a model that involves a single chemotactic substance [30], and

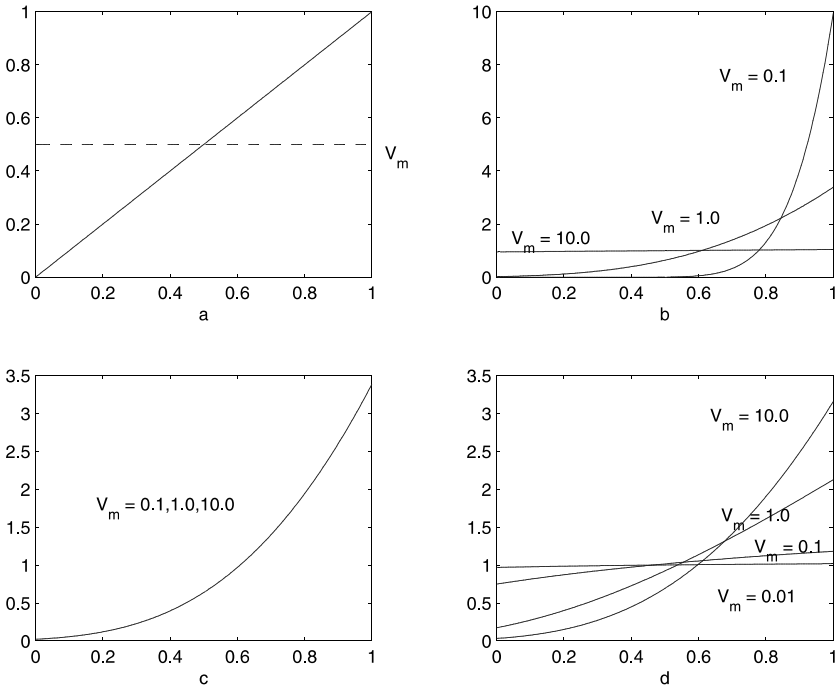


Fig. 9. Cell density response to a single gradient, while another attractant is fixed at a uniform level. (a) Chemical concentrations for u , solid line, and v dashed line, concentration of v determined by V_m . (b) Cell densities under Type 1 sensitivities, (c) cell densities under Type 2 sensitivities, (d) cell densities under Type 3 sensitivities

we suggest that this may be applicable in the context of animal coat markings. The application to bacterial chemotaxis shows how signals may be filtered such that very low levels of one stimulus can be detected in the presence of large gradients in a second stimulus. We have also shown that certain types of sensitivity laws favour robust patterning.

The patterns determined by the mechanism presented here derive from the local interpretation by cells of positional information provided by the nonuniform morphogen distribution. Because cells respond by moving, this leads to global patterning and in essence, a non-local interpretation of the positional information. This is in contrast to other models that do not involve chemotaxis, in which the complex patterns are obtained via the superposition of two linearly unstable modes [34,26] and the response is strictly local. These models can also generate complex patterns, but the one presented here is simpler: we rely on a single pattern generator (the reaction-diffusion mechanism) to create a spatially heterogeneous field and it is the subsequent interpretation of the field that forms the complex patterning. An important question that modeling alone cannot answer is what mechanisms are used in a particular context.

7. Appendix

We obtain analytical approximations for time independent solutions to the model below using standard bifurcation analysis (see, for example, Fife (1979) or Grindrod (1993)). On the scaled one-dimensional domain $[0, \pi]$ the model is given by:

$$\frac{\partial u}{\partial t} = \frac{\partial^2 u}{\partial x^2} + \gamma^2 (\delta - \kappa u - uv^2), \tag{64}$$

$$\frac{\partial v}{\partial t} = d \frac{\partial^2 v}{\partial x^2} + \gamma^2 (\kappa u + uv^2 - v), \tag{65}$$

with given initial conditions and zero flux at the boundaries. The parameter γ corresponds to a scaling of both spatial *and* temporal scales.

The homogeneous steady state solution for (64)–(65) is given by $(u_0, v_0) = \left(\frac{\delta}{\kappa + \delta^2}, \delta\right)$. We define $\mathbf{f}(u, v) = \gamma^2 \begin{pmatrix} \delta - \kappa u - uv^2 \\ \kappa u + uv^2 - v \end{pmatrix}$. The dispersion relation, obtained by looking for solutions of the form $\exp(\lambda t + i k x)$ for the system linearized around the steady state (u_0, v_0) , is given by

$$(\lambda(k^2))^2 + a(k^2)\lambda(k^2) + b(k^2) = 0, \tag{66}$$

where,

$$a(k^2) = (d + 1)k^2 + \gamma^2 (\kappa + v_0^2 + 1 - 2u_0v_0), \tag{67}$$

$$b(k^2) = dk^4 + \gamma^2 k^2 \left(1 - 2u_0v_0 + d(\kappa + v_0^2)\right) + \gamma^4 (\kappa + v_0^2). \tag{68}$$

Examination of the dispersion relation, Equation (66), demonstrates that eigenvalues have positive real part for $b < 0$, where b is determined by Equation (68). Algebraic manipulation of (68) gives $b = 0$ when:

$$d = \frac{\gamma^2 (2u_0v_0 - 1)k^2 - \gamma^4 (\kappa + v_0^2)}{k^2 (k^2 + \gamma^2 (\kappa + v_0^2))}, \tag{69}$$

which is positive for $k^2 > \frac{\gamma^2(\kappa + v_0^2)}{2u_0v_0 - 1}$. We take d as our bifurcation parameter. We let $k = j \in \mathbf{Z}$ and define d^* to be the solution of Equation (69). Assume, as d is decreased, that stability of the homogeneous solution is lost to the j^{th} mode first. Setting $d = d^* - \epsilon^2$, for ϵ small, we consider solutions (u, v) of the form:

$$\begin{pmatrix} u \\ v \end{pmatrix} = \begin{pmatrix} u_0 \\ v_0 \end{pmatrix} + \sum_{n=1}^{\infty} \epsilon^n \begin{pmatrix} u_n \\ v_n \end{pmatrix}. \tag{70}$$

and expand \mathbf{f} as a Taylor series in powers of ϵ .

Let \underline{L} be the differential operator:

$$\underline{L}\mathbf{w} = \begin{pmatrix} \frac{\partial^2}{\partial x^2} - \gamma^2 (\kappa + v_0^2) & -2\gamma^2 u_0 v_0 \\ \gamma^2 (\kappa + v_0^2) & d^* \frac{\partial^2}{\partial x^2} + \gamma^2 (2u_0 v_0 - 1) \end{pmatrix} \mathbf{w} \tag{71}$$

for suitable functions $\mathbf{w} : \mathbf{R}^2 \rightarrow \mathbf{R}$. We further define the matrix \underline{L}_j by the action of \underline{L} on terms of the form $\cos jx$.

At $O(\epsilon)$:

$$\underline{L} \begin{pmatrix} u_1 \\ v_1 \end{pmatrix} = 0 \quad \text{and} \quad u_{1x}, v_{1x} = 0 \quad \text{at} \quad x = 0, \pi. \tag{72}$$

This has a solution,

$$\begin{pmatrix} u_1 \\ v_1 \end{pmatrix} = A \begin{pmatrix} u^* \\ v^* \end{pmatrix} \cos jx, \tag{73}$$

where $(u^*, v^*)^T$ is an eigenvector parallel to

$$\begin{pmatrix} u^* \\ v^* \end{pmatrix} = \begin{pmatrix} 2\gamma^2 u_0 v_0 \\ -j^2 - \gamma^2 (v_0^2 + \kappa) \end{pmatrix}, \tag{74}$$

and A is a constant to be determined.

The solution to $O(\epsilon^2)$ is determined uniquely up to the constant B,

$$\begin{pmatrix} u_2 \\ v_2 \end{pmatrix} = -\frac{MA^2}{\gamma^2(v_0^2 + \kappa)} \begin{pmatrix} 1 \\ 0 \end{pmatrix} + B \begin{pmatrix} u^* \\ v^* \end{pmatrix} \cos jx + \frac{MA^2}{Q} \begin{pmatrix} -4j^2 d^* - \gamma^2 \\ 4j^2 \end{pmatrix} \cos 2jx. \tag{75}$$

where

$$M = \frac{\gamma^2}{2} (u_0 v^{*2} + 2u^* v^* v_0), \tag{76}$$

$$Q = 16d^* j^4 + 4j^2 \gamma^2 (d^* (v_0^2 + \kappa) + 1 - 2u_0 v_0) + \gamma^4 (\kappa + v_0^2) \tag{77}$$

At $O(\epsilon^3)$:

$$\underline{L} \begin{pmatrix} u_3 \\ v_3 \end{pmatrix} = \gamma^2 (2u_0 v_1 v_2 + 2v_0 (u_1 v_2 + u_2 v_1) + u_1 v_1^2) \begin{pmatrix} 1 \\ -1 \end{pmatrix} + v_{1xx} \begin{pmatrix} 0 \\ 1 \end{pmatrix} = \Psi. \tag{78}$$

The Fredholm Alternative (cf. [11]) states that the above equation has a solution if and only if Ψ is orthogonal to solutions of the adjoint equation. This gives,

$$0 = \frac{v}{(\mu - v) \gamma^2} \int_0^\pi v_{1xx} R \cos jx \, dx + \int_0^\pi (2u_0 v_1 v_2 + 2v_0 (u_1 v_2 + u_2 v_1) + u_1 v_1^2) \times R \cos jx \, dx. \tag{79}$$

where R is a constant and (μ, v) is an eigenfunction of \underline{L}^t corresponding to j^2 . This is parallel to

$$\begin{pmatrix} \gamma^2 (v_0^2 + \kappa) \\ j^2 + \gamma^2 (\kappa + v_0^2) \end{pmatrix}.$$

We can evaluate the above to give:

$$A \left(A^2 - \frac{v^* v j^2}{2\gamma^2 C(\mu - \nu)} \right) = 0 \quad (80)$$

where

$$C = \left[\frac{2u_0 v^* M j^2}{Q} + \frac{2v_0 u^* M j^2}{Q} - \frac{v_0 v^* M}{\gamma^2 (v_0^2 + \kappa)} - \frac{2v_0 v^* M}{4Q} (4j^2 d^* + \gamma^2) + \frac{3u^* v^{*2}}{8} \right].$$

Equation (80) implies that as d decreases through the critical value, d^* , two non-trivial equilibria bifurcate from (u_0, v_0) according to:

$$\begin{pmatrix} u \\ v \end{pmatrix} = \begin{pmatrix} u_0 \\ v_0 \end{pmatrix} \pm \epsilon \left(\frac{v^* v j^2}{2\gamma^2 C(\mu - \nu)} \right)^{1/2} \begin{pmatrix} u^* \\ v^* \end{pmatrix} \cos jx + O(\epsilon^2). \quad (81)$$

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